

Inter-stimulus Interval Study for the Tactile Point-pressure Brain-computer Interface

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Abstract—The paper presents a study of an inter-stimulus interval (ISI) influence on a tactile point-pressure stimulus-based brain–computer interface’s (tpBCI) classification accuracy. A novel tactile pressure generating tpBCI stimulator is also discussed, which is based on a three-by-three pins’ matrix prototype. The six pin-linear patterns are presented to the user’s palm during the online tpBCI experiments in an oddball style paradigm allowing for “the aha-responses” elucidation, within the event related potential (ERP). A subsequent classification accuracies’ comparison is discussed based on two ISI settings in an online tpBCI application. A research hypothesis of classification accuracies’ non-significant differences with various ISIs is confirmed based on the two settings of 120 ms and 300 ms, as well as with various numbers of ERP response averaging scenarios.

I. INTRODUCTION

A brain–computer interface (BCI) is a technology that uses only the central nervous system signals (brainwaves) of paralyzed or locked-in syndrome (LIS) patients [1] to create a new communication channel with others or to control external devices without depending on any muscle activity [2], [3]. The BCI technology has provided a support already to patients’ life improvement who suffer from severe paralysis due to diseases like an amyotrophic lateral sclerosis (ALS) [2]. The contemporary BCI applications rely mostly on a visual mode, which generates the most reliable event related potentials (ERP) so far [4]. However, many LIS patients in the advanced disease stages often lose their ability to control reliably even their eyeball focusing or movement abilities [1], [5], and therefore they need the alternative options for BCI-enabled communication.

The successful alternative options have been developed recently to utilize spatial auditory [4], [6] or tactile (somatosensory) modes [5], [7]. Meanwhile, the tactile BCI seems to offer the superior communication options in comparison with the contemporary visual and auditory modes in case of LIS patients [1], [8].

We present results of a followup study with an extended number to ten subjects comparing to our previous reports [9], [10]. We test the tactile point-pressure stimulus-based brain–computer interface (tpBCI) using stimuli generated by a matrix of small solenoids (see Figure 1). The tpBCI device

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can generate various patterns to be applied to possibly different body areas, and therefore it could be adopted to many patient symptoms. The presented approach allows for faster and more precise delivery of tactile pressure stimuli comparing to the previously proposed vibrotactile stimulator-based approaches [5], [7] and it is not limited to finger tips only [8].

The goal of this study is to compare and test the performance (BCI classification accuracy) of the novel tpBCI paradigm [9], [10] in function of two inter-stimulus interval (ISI) settings. Namely the ISI equal to 300 ms (a very easy for the users) and 120 ms (a harder case due to fast repetition of the presented pin-pressure patterns and larger overlap of the brainwave ERPs).

Results obtained with ten healthy users’ offline analysis with stepwise linear discriminant analysis (SWLDA) classifier [11] and five different averaging settings are analyzed for statistical significance.

From now on the paper is organized as follows. In the next section we present methods used and developed in order to capture, process and classify the brainwave response in application to the proposed tpBCI. Offline EEG analysis results together with conclusions summarize the paper.

II. METHODS

A. Tactile Pin-pressure Stimulus Device

The tactile stimuli were delivered as light pin-pressure patterns generated by a portable computer with a program developed by our team on the ARDUINO UNO microcontroller board managed from our visual programming application designed in MAX 6 [12]. Each tactile stimulus pattern was generated via the tactile pressure device composed of nine solenoids arranged in the 3×3 matrix as depicted in Figure 1. The binary outputs from the ARDUINO UNO micro-controller board were amplified by a multichannel amplifier (battery driven for user’s safety) developed also by our team. There were six linear patterns of tactile pressure stimuli delivered in random order to the user fingers (for details please refer to [9]) in order to elicit P300 brainwave responses in an oddball style paradigm [2].

The solenoids generated quick, 100 ms long, light pin-pressure with inter-stimulus intervals (ISI) of 120 ms and 300 ms in two settings as explained in Table I with experimental condition details. The two different ISI setups were tested in order to evaluate a possible impact of the fast stimulation repetitions on user’s BCI performance (the resulting BCI accuracy) in five different averaging scenarios.

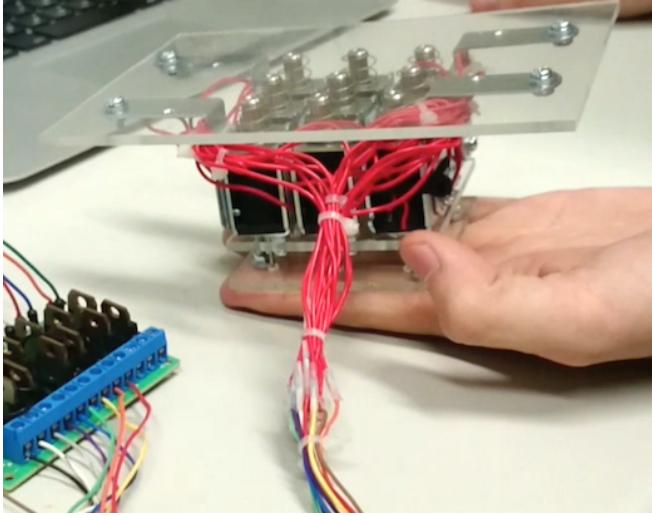


Fig. 1. The tactile pressure generator composed of nine solenoids placed on the user's dominant plastic glove covered hand. The solenoids created six linear pressure patterns.

B. EEG Experiments

During the EEG experiments, the users placed the tactile stimulus generator on their dominant hand's fingers with a plastic glove to prevent any spurious electric current interferences possibly originating from the device. The users responded mentally by confirming/counting only to the instructed patterns while ignoring the others. The training instructions were presented visually by means of the MAX 6 [12] programmed display designed by our team as depicted in Figure 2.

In the online BCI experiments (similarly as in our previous study [9]) the EEG signals were captured with a portable EEG amplifier system g.USBamp from g.tec Medical Instru-

TABLE I

CONDITIONS AND DETAILS OF THE TPBCI EEG EXPERIMENT

Condition	Detail
Number of users	10
Tactile stimulus length	100 ms
Inter-stimulus-interval (ISI)	120 and 300 ms
EEG recording system	g.USBamp active wet electrodes
Number of the EEG channels	8
EEG electrode positions	Cz, Cpz, P3, P4, C3, C4, CP5, and CP6
Reference electrode	Behind the user's left earlobe
Ground electrode	On the forehead(FPz)
Stimulus generator	3 × 3 pressure pins matrix
Number of trials for each user	5

ments, Austria. Eight active wet EEG electrodes were used to capture brainwaves with attentional modulation elucidated, within the event related potentials (ERPs), the so-called "aha" or P300-responses [2]. The EEG electrodes were attached to the head locations *Cz*, *Cpz*, *P3*, *P4*, *C3*, *C4*, *CP5*, and *CP6* as in 10/10 intentional system [13]. A reference electrode was attached to a left earlobe and a ground electrode on the forehead at *FPz* position respectively. The experimental details are summarized in Table I.

The users were requested to limit their eye-blanks and body muscle movements to avoid electromagnetic and electromyographic interferences. The unavoidable eye-blanks were identified within the ERPs and removed with a threshold setting of 80 μ V. All EEG experiments were conducted in the Life Science Center of TARA, University of Tsukuba, Japan. The details of the experimental procedures and the research targets of the tpBCI paradigm were explained in detail to the seven human users, who agreed voluntarily to participate in the study. The electroencephalogram (EEG) tpBCI experiments were conducted in accordance with *The World Medical Association Declaration of Helsinki - Ethical Principles for Medical Research Involving Human Subjects*. The experimental procedures were approved and designed in agreement with the ethical committee guidelines of the Faculty of Engineering, Information and Systems at University of Tsukuba, Tsukuba, Japan (experimental permission no. 2013R7).

Ten subjects participated in two studies with various ISI settings for tBCI's stimulus speed and difficulty evaluation. The average age of the users was of 24.8 years old (standard deviation of 3.8 years old; ten men).

C. EEG Signals Processing and Classification

The EEG signals were recorded and preprocessed online by an in-house extended BCI2000 application [14] and segmented ("epoched") as features drawn from ERP intervals of 0 ~ 900 ms. A common average reference (CAR) filter were also applied to the segmented signals. The sampling rate was set to 512 Hz, the high pass filter at 0.1 Hz, and the low pass filter at 40 Hz. The ISI were of 120 ms or 300 ms

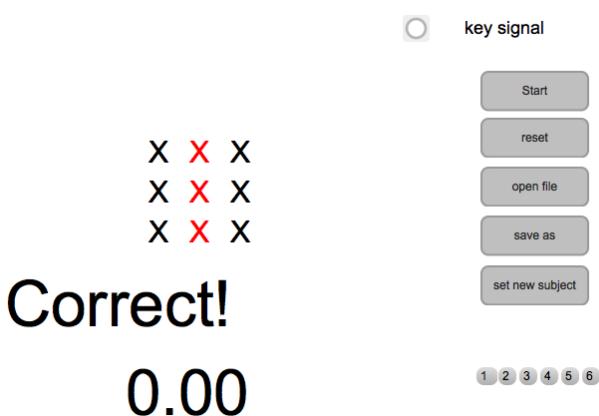


Fig. 2. The visual instruction screen presented to the users during the experiments programmed in MAX 6 [12]. The red \times symbols inform about the pattern shape to be attended by a user in each SWLDA training experimental run.

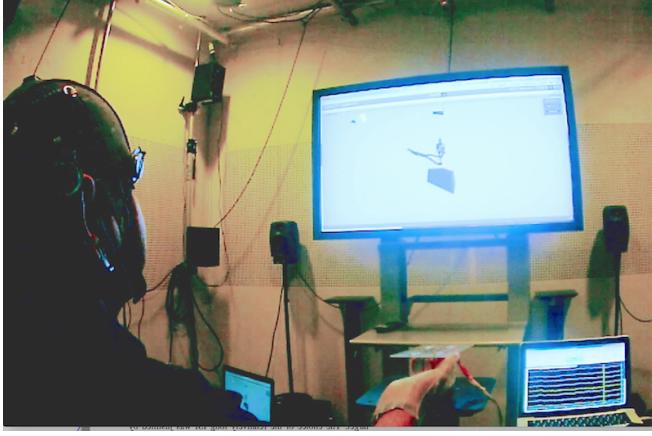


Fig. 3. A screenshot from a demo video available online [3] presenting single trial based online tpBCI application to a computer game-based real-time virtual agent walking control (see the last part of the online video).

in two different experimental runs, and each tactile pressure stimulus duration was of 100 ms. Each user performed two sessions of selecting the six patterns (a spelling of a sequence of six digits associated with each tactile pressure pattern). Each target was presented five times in a random series with the remaining non-targets. We performed offline analysis of the collected online EEG datasets in order to test a possible influence of the two ISI settings on the tpBCI accuracy (compare ERP results in Figures 4 and 5 depicting an impact of faster ISI on the ERP shapes and areas under the curve (AUC) based discriminative latencies). The stepwise linear discriminant analysis (SWLDA) [11] classifier was applied next, with features drawn from the 0 ~ 900 ms ERP interval, with removal of the least significant input features, having $p > 0.15$, and with the final discriminant function restricted to contain a maximum of 60 features.

A screenshot from an online virtual reality application [10] of the discussed paradigm demonstrating single trial-based tpBCI operation is presented in Figure 3. A demonstration video is also available online at [3].

III. RESULTS

The results of the SWLDA in comparison of the two ISI settings have been summarized in Table II. The results were slightly better for the longer ISI of 300 ms, yet this observation was not confirmed with a Wilcoxon rank sum test of a statistical significance for equal medians (the distributions were not normal).

We concluded that the analysis of EEG data obtained from the ten healthy subjects did not confirm significantly that shorter ISI, causing a larger experimental difficulty, would sabotage the tpBCI accuracy as summarized in Table II.

IV. CONCLUSIONS

The aim of this study was to test the ISI variability impact on the BCI classification accuracy results in various brainwave averaging scenarios of the proposed tactile pin-pressure BCI paradigm. The offline results obtained with

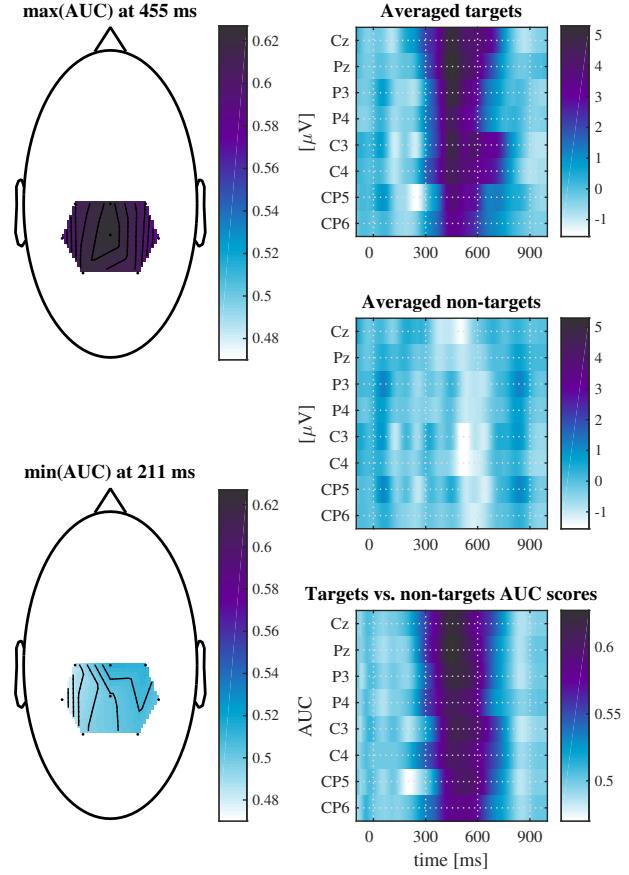


Fig. 4. A summary of the grand mean averaged ERPs from experiments with $ISI = 300$ ms presented in left panels. The very clear P300 target responses are depicted with white shades. The right bottom panel presents an area under the curve (AUC) discriminability analysis. The left head topographical maps present the electrode locations together with maximum and minimum AUC scores.

the SWLDA classifier did not show significant differences, although the median tpBCI classification results for ISI of 300 ms seemed to be higher.

The results are very promising for future online applications with patients suffering from LIS allowing for speeding up the BCI stimuli presentation without significant classification drop danger.

The approach presented shall help, if not to reach the goal, to get closer to our objective of the more user friendly tactile BCI design, which would fit those users with bad, or disabled, vision and hearing. Thus, we can expect that patients suffering from LIS will be able to use the appropriate BCI interfaces, according to their intact sensory modalities, more efficiently and comfortably to restore their basic communication needs.

Still there remains a long path to go before providing the effective and comfortable tactile BCI end-user solution, yet our research has progressed toward this goal as presented in this paper.

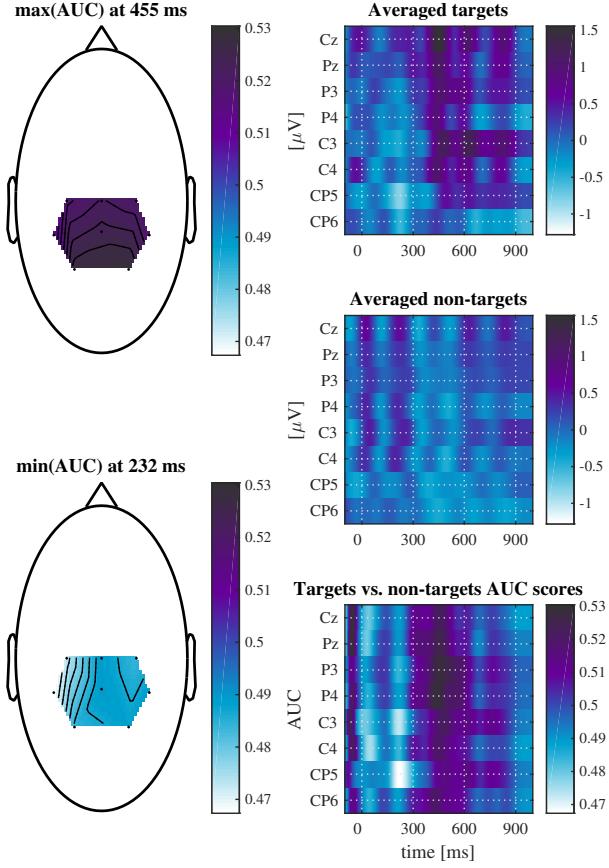


Fig. 5. A summary of the grand mean averaged ERPs from experiments with $ISI = 120$ ms presented in left panels. The very clear P300 target responses are depicted with white shades. The right bottom panel presents an area under the curve (AUC) discriminability analysis. The left head topographical maps present the electrode locations together with maximum and minimum AUC scores.

TABLE II
SINGLE TO FIVE TRIALS BASED TPBCI MEDIAN ACCURACY AND FIRST QUARTILE (25^{th} -PERCENTILE) RESULTS, WITHOUT STATISTICAL SIGNIFICANCES AT A LEVEL OF $p \gg 0.05$ AS TESTED WITH THE WILCOXON RANK SUM TEST FOR EQUAL MEDIANS

Mean tpBCI accuracy and standard deviation results of ten subjects from experiments with $ISI = 300$ ms		
Number of averages	Median accuracy	Data first quartile (25^{th} -percentile)
1	41.5%	21.0%
2	33.0%	21.0%
3	50.0%	33.0%
4	50.0%	33.0%
5	66.5%	37.3%

Mean tpBCI accuracy and standard deviation results of ten subjects from experiments with $ISI = 120$ ms		
Number of averages	Median accuracy	Data first quartile (25^{th} -percentile)
1	17.0%	9.0%
2	33.0%	17.0%
3	33.0%	25.0%
4	33.0%	25.0%
5	33.0%	25.0%

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